The accuracy of various radiographic modalities for implant therapy

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ABSTRACT

Aims and objectives

To investigate the dimensional accuracy of radiographic techniques utilized during implant therapy.

Design and Methods

Six dried human skulls were used to compare three dimensions in ten anatomical segments. Linear distances in-between metallic markers were measured and compared physically, and virtually on cone-beam computed tomography (CBCT) volumes, panoramic (PAN) and periapical (PA) radiographs. The angular distances along the curved arches of both jaws (connecting the upper metallic markers) were measured using cords. One-way ANOVA (p-value < 0.05) tests were executed to statistically analyze the mean differences between physical and virtual distances measured. The intra-class correlation coefficient (ICC) was used to analyze the level of consistency of observers.

Results

Statistically significant overall mean difference of all distances comparing physical and radiographic (CBCT, PAN, and PA), with the CBCT showed the least overall submillimeter discrepancy in the maxilla (M.D= -0.638 mm, SD= 0.203) and mandible (M.D=0.326 mm, SD=0.23).

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Overestimations exceeding a millimeter were found in maxilla (M.D=2.229 mm, SD=0.856) and mandible (M.D=3.832 mm, SD=1.272) of measurements performed on panoramic radiographs. Periapical radiographs exhibited an overall mean maxillary underestimation of -3.707 mm, (SD=1.31) and mandibular mean overestimation of 1.849 mm (SD=0.875).

Conclusion

CBCT demonstrated a superior submillimeter overall accuracy in comparison to periapical and panoramic radiographs. While PAN and PA presented with individual dimension precision (submillimeter difference), the overall mean of difference for these modalities was inferior when compared with CBCT. CBCT showed superior dimensional stability and thus it is recommended during implant planning phases.

Keywords

CBCT, accuracy, panorama, implant, periapical.

INTRODUCTION

Radiographic assessment during various phases of dental implant therapy has become indispensable. Panoramic radiography is the most popular and the backbone radiographical procedure prescribed during daily practice and different phases of implant therapy. On the other hand, the new era introduced by the cone-beam computed tomography (CBCT) aided to reform the treatment planning approaches and the diagnostic abilities of the practitioners. CBCT allows for dimensionally accurate 3D imaging 7 that facilitates the aid of various applications e.g., computerguided surgical procedures.

Each radiographic modality can offer both advantages and drawbacks, but providing precise and reproducible dimensions of the anatomical site of interest is a vital requirement. 9,10 A submillimetre radiographic measurement error is still tolerable during implant treatment according to multiple reports. 11,12 Inconsistent evidence was found on the ideal radiographic modality (particularly from a dimensional accuracy perspective) that is most suitable to be used during the planning phase. 10

The assessment of the vertical bone dimensions for implant purposes on the panoramic radiographs, especially in non-complex cases was reported. 3,10,13-18 On the contra-

ry, other reports¹⁹⁻²³ provided opposite evidence as these radiographs may predispose risks due to possible dimensional inaccuracies encountered (particularly if no magnification factors are considered).

As the maxilla and mandible are curved and in multidimensions, the presentation of these structures on a certain radiograph should be evaluated when a dimensional analysis is to be carried out for implant planning purposes; this indicates the consideration of angular measurements in certain anatomical regions (where applicable).

The authors presume that reproducing 2D radiographic dimensions on 3D physical structures (i.e., jaws) may predispose inaccuracies. The current investigation tries to add to the pool of evidence on the accuracy of linear and physical angular measurements (for implant planning purposes) in various radiographic modalities.

MATERIAL AND METHODS

Six dried human skulls (gender and ethnicity have been neglected) were collected from the Division of Clinical Anatomy, Faculty of Medicine, Stellenbosch University (Cape Town, South Africa) after obtaining ethical approval for degree purposes (Number: BM19/1/20, University of the Western Cape, South Africa). The adult-size skulls were provided with fully edentulous maxilla and mandible, and with the calvarium cut off. Metallic bearing balls of known diameter (4.5mm) were fixed directly on the mandibular and maxillary bone surfaces using a rigid sticky wax.

Five regions (segments) in each jaw were selected as follows: A-segment (anteriorly), M/C-segment (M: mental foramen region in the mandible and C: Canine segment in the maxilla), and P-segment (posteriorly). Each segment in the mandible contains three balls aligned in a triangular pattern (Y-ball placed on the top of the alveolar ridge, and two parallel balls with one on the buccal (X-ball) and lingual/palatal surfaces (Z-ball)). In the maxilla, only marker balls (X and Y) were placed (Figure 1).

Hight (DV: distance vertical), length (DH: distance horizontal), and width (DLA, DLP, DUA, DUP: distance lower/upper anterior/posterior) between these balls were measured physically by a digital caliber (Mastercraft®, South Africa) with 0,03 mm accuracy, and 0,01 mm repeatability.

The caliber readings were confirmed manually using a ruler before the analysis of every skull. Finally, thin nylon cords were fixed directly on the upper cortex of the ridge between the Y balls (conforming to the anatomy of the bone) and then measured by the caliber's ruler.

The skulls were mounted on a tripod during examinations with the mandibles that were supported with uniformly-sized sponges placed under the mandibular angles (bilaterally) simulating an ideal radiographic position. A uniform level between the left and right sides of the mandible was ensured using a combination square with a spirit level which also acted as a physical upper limit (tangent) for DV measurements.

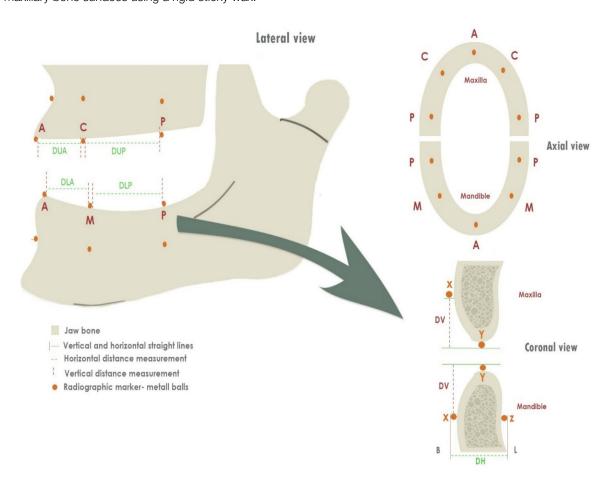


Figure 1. Measurements' diagram (Reprinted from Beshtawi, 2021). 40

The ideal radiographic position during CBCT and panoramic examinations were ensured with the aid of the units' positioning laser markers (Figure 2).

Parallel radiographic technique (with the aid of film holders) was employed during intraoral periapical examinations. The corresponding radiographic measurements were carried out virtually (Figure 3).





Figure 2. X-ray machines that were used (A) CBCT, (B) panoramic, and (C) periapical x-ray machines.

Table I shows the models ofx-ray machines utilized, the exposure parameter selected, and the distances measured for each modality.

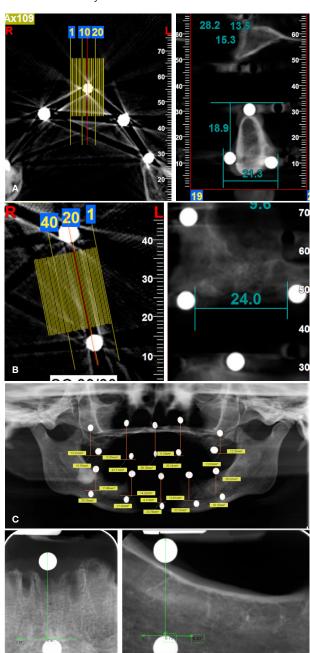


Figure 3. Virtual measurements captured on CBCT volumes (A&B), panoramic (C), periapical (D) radiographs..

Modality	Model	Exposure parameters	Distances measured (maxilla and mandible)
PA	 Phosphor plates. Plate scanner: SOREDEX® DIGORA™ Optime (Kavo/ Soredex®, Helsinki, Finland). Desktop user-grade monitor. 	70 kVp, 2 mAs	DV
PAN	 Sirona® Orthophos XG3 (Dentsply Sirona, Bernsheim, Germany). Desktop user-grade monitor. 	64 kVp, 112 mAs	DV, DLA, DLP, DUP, and DUA
СВСТ	 Newtom® VGi (CEFLA s.c., Imola, Italy) Barco® (Kortrijk, Belgium) Eonis 22" medical monitor 2MP (1920×1080 pixels). 	"Full scan" mode 110 kVp, 1-10 mA	DV, DH, DLA, DLP, DUP, and DUA.

Key - PA: periapical, PAN: panoramic radiograph, CBCT: cone beam computed tomography, DV: distance vertical, DH: distance horizontal, DLA: distance lower anterior, DLP: distance lower posterior, DUP: distance upper posterior, and DUA: distance upper anterior.

			asareme	nts), (Reprint Mean value	ou nom	CBCT vs.	_	PA vs.						Mean value		CBCT vs.	Pan vs	PA vs
				(SD)			Physical	Physical	Maxilla					Wedir Value		Physical		
	i		Physical	15.02 (3.4)	M.D	1.18	4.87	2.252					Physical	17.67 (1.6)	M.D	-0.671	1.155	-3.786
			CBCT	16.2 (3.1)	SD	-2.02	-2.02	2.02					CBCT	17 (2.0)	SD	1.07	1.07	1.07
		DV	PAN	19.89 (3.9)	P.V	1	0.154	1				DV	PAN	18.83 (2.4)	P.V	1	1	0,012
			PA	17.27 (3.6)									PA	13.89 (1.2)				
			D	10.50 (1.0)		0.000												
Doint	nt p	DII	Physical	18.59 (1.9)	M.D	0.362					Point p							
0	2	DH	CBCT	18.95 (2.1)	SD P.V	-1.17 0.764					Po							
					r.v	0.764												
			Physical	23.19 (3.9)	M.D	-0.738	1.63						Physical	22.29 (3.3)	M.D	698	1.55	
		DLP	CBCT	22.45 (3.8)	SD	-2.21	-2.21					DUP	CBCT	21.6 (3.2)	SD	1.99	1.99	
			PAN	24.82 (3.7)	P.V	1	1			S			PAN	23.85 (3.8)	P.V	1	1	
Ę			Physical	17.22 (4.2)	M.D	1.582	6.692	2		RHS			Physical	24.25 (4.1)	M.D	-0.15	3.97	-4.57
			CBCT	18.8 (4.4)	SD	-2.64	-2.64	-2.64					CBCT	24.1 (3.9)	SD	2.41	2.41	2.41
		DV	PAN	23.91 (5.3)	P.V	1	0.118	1				DV	PAN	28.22 (4.8)		1	0.689	0.43
			PA	19.22 (4.2)									PA	19.69 (3.8)				
	5										o			, ,				
O'Daint MA/C	Ž		Physical	19.02 (0.9)	M.D	0.127					Point M/C							
i	ē	DH	CBCT	19.15 (0.9)	SD	-0.538					Poin							
ľ					P.V	0.819					Ť.							
			Physical	18.63 (3.8)	M.D	-0.927	0.907						Physical	16.68 (3.9)	M.D	-0.73	1.32	
		DLA	CBCT	17.7 (3.8)	SD	-2.3	-2.3					DUA	CBCT	15.95 (3.9)	SD	2.39	2.39	
			PAN	19.53 (4.4)	P.V	1	1						PAN	18 (4.6)	P.V	1	1	
Н			Physical	16.05(4.41)	M.D	2.047	7.50	2.15					Physical	24.92 (2.5)	MD	0.227	6.055	-0.83
			CBCT	18.1(5.50)	SD	-3,036	7.56 -3,036	-3,036					CBCT		SD	2.07	2.07	2.07
		DV	PAN	23.61(6.5)	P.V	1		1				DV	PAN	30.97 (4.1)		1	0.05	1
<	<		PA	18.2(4.27)	1.0	1	0.13			ē	4		PA	24.09 (4.7)	1.0	'	0.00	,
Center	E O		171							Center	Point A		170	24.00 (4.17)				
ه (ì		Physical	21.44 (1.6)	M.D	0.31				Ŭ	Ť.							
		DH	CBCT	21.75 (1.5)	SD	-0.91												
					P.V	0.74												
			Physical	15.5 (3.4)	M.D	0.7	5.238	1.56					Physical	21.34 (2.4)	M.D	-0.293	3.801	-3.77
		DV	CBCT	16.2 (3.6)	SD	-2.29	-2.29	-2.29					CBCT	21.05 (2.5)	SD	1.56	1.56	1.56
								4				D1/						
		DV	PAN	20.74 (4.8)	P.V	1	0.199	1				DV	PAN	25.15 (3.1)	P.V	1	0.147	0.15
		DV	PAN PA	20.74 (4.8) 17.06 (3.9)	P.V	1	0.199	ı				DV		25.15 (3.1) 17.57 (2.8)	P.V	1	0.147	0.15
٥	2	DV	PA	17.06 (3.9)			0.199	ı			رد	DV			P.V	1	0.147	0.15
- M/C	T M/C		PA Physical	17.06 (3.9) 19.46 (0.7)	M.D	0.242	0.199	1			nt M/C	DV			P.V	1	0.147	0.15
Doing M/C	Point M/C	DH	PA	17.06 (3.9)	M.D SD	0.242	0.199	1			Point M/C	DV			P.V	1	0.147	0.15
Doint M/C	Point M/C		PA Physical	17.06 (3.9) 19.46 (0.7)	M.D	0.242	0.199	1			Point M/C	DV			P.V	1	0.147	0.150
O M toil	Point M/C	DH	PA Physical CBCT Physical	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2)	M.D SD	0.242 -0.46 0.611 -0.698	1.31	1			Point M/C		PA Physical	17.57 (2.8) 16.59 (3.9)		-0.988	1.465	0.15
O'M triod	Point M/C		PA Physical CBCT Physical CBCT	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0)	M.D SD P.V M.D SD	0.242 -0.46 0.611 -0.698 -2.31		1			Point M/C	DV	PA Physical CBCT	17.57 (2.8) 16.59 (3.9) 15.6 (3.7)	M.D SD	-0.988 2.313	1.465 2.313	0.15
O'M toil G	Point M/C	DH	PA Physical CBCT Physical	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2)	M.D SD P.V M.D	0.242 -0.46 0.611 -0.698	1.31				Point M/C		PA Physical	17.57 (2.8) 16.59 (3.9)	M.D SD	-0.988	1.465	0.150
	Point M/C	DH	PA Physical CBCT Physical CBCT	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0)	M.D SD P.V M.D SD	0.242 -0.46 0.611 -0.698 -2.31	1.31 -2.31	1.28		HS	Point M/C		PA Physical CBCT	17.57 (2.8) 16.59 (3.9) 15.6 (3.7)	M.D SD P.V	-0.988 2.313	1.465 2.313	
CH3	Point M/C	DH	PA Physical CBCT Physical CBCT PAN	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0) 18.36 (3.8)	M.D SD P.V M.D SD P.V	0.242 -0.46 0.611 -0.698 -2.31	1.31 -2.31 1			LHS	Point M/C	DUA	Physical CBCT PAN	17.57 (2.8) 16.59 (3.9) 15.6 (3.7) 18.05 (4.3)	M.D SD P.V M.D	-0.988 2.313	1.465 2.313 1	-5.57
	Point M/C	DH	PA Physical CBCT Physical CBCT PAN Physical	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0) 18.36 (3.8) 13.41 (2.92)	M.D SD P.V M.D SD P.V	0.242 -0.46 0.611 -0.698 -2.31 1	1.31 -2.31 1 3.94	1.28		КНЗ	Point M/C		Physical CBCT PAN Physical	17.57 (2.8) 16.59 (3.9) 15.6 (3.7) 18.05 (4.3) 15.36 (3.2)	M.D SD P.V M.D SD	-0.988 2.313 1	1.465 2.313 1	-5.5° 2.08
	Point M/C	DH	PA Physical CBCT Physical CBCT PAN Physical CBCT	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0) 18.36 (3.8) 13.41 (2.92) 13.9 (2.68)	M.D SD P.V M.D SD P.V M.D SD	0.242 -0.46 0.611 -0.698 -2.31 1 0.49 -1.83	1.31 -2.31 1 3.94 -1.83	1.28		CHS	Point M/C	DUA	Physical CBCT PAN Physical CBCT	17.57 (2.8) 16.59 (3.9) 15.6 (3.7) 18.05 (4.3) 15.36 (3.2) 13.55 (3.1)	M.D SD P.V M.D SD	-0.988 2.313 1 -1.807 2.08	1.465 2.313 1 -0.777 2.08	-5.57 2.08
S.		DH	PA Physical CBCT Physical CBCT PAN Physical CBCT PAN PA	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0) 18.36 (3.8) 13.41 (2.92) 13.9 (2.68) 17.35 (3.52) 14.68 (3.435)	M.D SD P.V M.D SD P.V M.D SD P.V	0.242 -0.46 0.611 -0.698 -2.31 1 0.49 -1.83	1.31 -2.31 1 3.94 -1.83	1.28		SHT		DUA	Physical CBCT PAN Physical CBCT PAN	17.57 (2.8) 16.59 (3.9) 15.6 (3.7) 18.05 (4.3) 15.36 (3.2) 13.55 (3.1) 14.58 (3.7)	M.D SD P.V M.D SD	-0.988 2.313 1 -1.807 2.08	1.465 2.313 1 -0.777 2.08	-5.57 2.08
S.		DH DLA	PA Physical CBCT Physical CBCT PAN Physical CBCT PAN PA Physical	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0) 18.36 (3.8) 13.41 (2.92) 13.9 (2.68) 17.35 (3.52) 14.68 (3.435) 19.56 (2.2)	M.D SD P.V M.D SD P.V M.D SD P.V	0.242 -0.46 0.611 -0.698 -2.31 1 0.49 -1.83 1	1.31 -2.31 1 3.94 -1.83	1.28		THS		DUA	Physical CBCT PAN Physical CBCT PAN	17.57 (2.8) 16.59 (3.9) 15.6 (3.7) 18.05 (4.3) 15.36 (3.2) 13.55 (3.1) 14.58 (3.7)	M.D SD P.V M.D SD	-0.988 2.313 1 -1.807 2.08	1.465 2.313 1 -0.777 2.08	-5.57 2.08
		DH	PA Physical CBCT Physical CBCT PAN Physical CBCT PAN PA	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0) 18.36 (3.8) 13.41 (2.92) 13.9 (2.68) 17.35 (3.52) 14.68 (3.435)	M.D SD P.V M.D SD P.V M.D SD P.V	0.242 -0.46 0.611 -0.698 -2.31 1 0.49 -1.83 1	1.31 -2.31 1 3.94 -1.83	1.28		CHS	Point P Point M/C	DUA	Physical CBCT PAN Physical CBCT PAN	17.57 (2.8) 16.59 (3.9) 15.6 (3.7) 18.05 (4.3) 15.36 (3.2) 13.55 (3.1) 14.58 (3.7)	M.D SD P.V M.D SD	-0.988 2.313 1 -1.807 2.08	1.465 2.313 1 -0.777 2.08	-5.5° 2.08
S.		DH DLA	PA Physical CBCT Physical CBCT PAN Physical CBCT PAN PA Physical	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0) 18.36 (3.8) 13.41 (2.92) 13.9 (2.68) 17.35 (3.52) 14.68 (3.435) 19.56 (2.2) 19.9 (2.2)	M.D SD P.V M.D SD P.V M.D SD P.V	0.242 -0.46 0.611 -0.698 -2.31 1 0.49 -1.83 1	1.31 -2.31 1 3.94 -1.83 0.259	1.28		SHT		DUA	Physical CBCT PAN Physical CBCT PAN PA	17.57 (2.8) 16.59 (3.9) 15.6 (3.7) 18.05 (4.3) 15.36 (3.2) 13.55 (3.1) 14.58 (3.7) 9.78 (4.3)	M.D SD P.V M.D SD P.V	-0.988 2.313 1 -1.807 2.08	1.465 2.313 1 -0.777 2.08	-5.57 2.08
S.		DH DLA	PA Physical CBCT PAN Physical CBCT PAN Physical CBCT PAN CBCT PAN PA Physical CBCT PAN PA Physical	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0) 18.36 (3.8) 13.41 (2.92) 13.9 (2.68) 17.35 (3.52) 14.68 (3.435) 19.56 (2.2) 19.9 (2.2)	M.D SD P.V M.D SD P.V M.D SD P.V M.D SD P.V M.D	0.242 -0.46 0.611 -0.698 -2.31 1 0.49 -1.83 1	1.31 -2.31 1 3.94 -1.83	1.28		THS		DUA DV	PA Physical CBCT PAN Physical CBCT PAN PA Physical	17.57 (2.8) 16.59 (3.9) 15.6 (3.7) 18.05 (4.3) 15.36 (3.2) 13.55 (3.1) 14.58 (3.7) 9.78 (4.3)	M.D SD P.V M.D SD P.V	-0.988 2.313 1 -1.807 2.08 1	1.465 2.313 1 -0.777 2.08 1	-5.57 2.08
S.		DH DLA	PA Physical CBCT Physical CBCT PAN Physical CBCT PAN PA Physical CBCT PAN PA CBCT CBCT CBCT	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0) 18.36 (3.8) 13.41 (2.92) 13.9 (2.68) 17.35 (3.52) 14.68 (3.435) 19.56 (2.2) 19.9 (2.2) 21.5 (5.1) 21.1 (5.2)	M.D SD P.V M.D SD P.V M.D SD P.V M.D SD P.V	0.242 -0.46 0.611 -0.698 -2.31 1 0.49 -1.83 1 0.34 -1.27 0.795 -0.452 -3.25	1.31 -2.31 1 3.94 -1.83 0.259	1.28		SHT		DUA	PA Physical CBCT PAN Physical CBCT PAN PA Physical CBCT CBCT CBCT	17.57 (2.8) 16.59 (3.9) 15.6 (3.7) 18.05 (4.3) 15.36 (3.2) 13.55 (3.1) 14.58 (3.7) 9.78 (4.3) 21.73 (2.9) 21.1 (2.7)	M.D SD P.V M.D SD P.V	-0.988 2.313 1 -1.807 2.08 1	1.465 2.313 1 -0.777 2.08 1	-5.57 2.08 0.086
S.		DH DLA	PA Physical CBCT PAN Physical CBCT PAN Physical CBCT PAN CBCT PAN PA Physical CBCT PAN PA Physical	17.06 (3.9) 19.46 (0.7) 19.7 (0.9) 17.05 (4.2) 16.35 (4.0) 18.36 (3.8) 13.41 (2.92) 13.9 (2.68) 17.35 (3.52) 14.68 (3.435) 19.56 (2.2) 19.9 (2.2)	M.D SD P.V M.D SD P.V M.D SD P.V M.D SD P.V M.D	0.242 -0.46 0.611 -0.698 -2.31 1 0.49 -1.83 1	1.31 -2.31 1 3.94 -1.83 0.259	1.28		SHT		DUA DV	PA Physical CBCT PAN Physical CBCT PAN PA Physical	17.57 (2.8) 16.59 (3.9) 15.6 (3.7) 18.05 (4.3) 15.36 (3.2) 13.55 (3.1) 14.58 (3.7) 9.78 (4.3)	M.D SD P.V M.D SD P.V	-0.988 2.313 1 -1.807 2.08 1	1.465 2.313 1 -0.777 2.08 1	-5.57 2.08

*Statistically significant difference, p < 0.05 , Negative values indicate underestimation while positive ones indicate overestimation.

M.D: measurement discrepancy, SD: standard deviation, P.V: p-value, RHS: right hand side, LHS: left hand side, PA: periapical, PAN: panoramic radiograph, CBCT: cone beam computed tomography, DV: distance vertical, DH: distance horizontal, DLA: distance lower anterior, DLP: distance lower posterior, DUP: distance upper posterior, and DUA: distance upper anterior.

A one-way ANOVA test was used to determine if there was a statistically significant difference between the physical and radiographic (CBCT, PAN, and PA) distances. Pairwise comparisons with Bonferroni correction were used to determine how large those differences were and to determine where those differences were.

If there were no statistically significant differences between the different modalities, then the two differences were deemed similar, as the p-value was greater than 0.05 and the confidence interval included zero. If the confidence interval included zero, this implied that at some stage the difference was zero and thus there was no difference in the estimation of the distance of the points between the physical point or any of the three modalities (CBCT, PAN, or PA). The mean measurement difference (M.D) was calculated in millimeters and using the following equation:

M.D=mean radiographic measurements – mean physical measurements

The intra-class correlation coefficient (ICC) was used to analyze the level of consistency of the results between the two observers. All the physical measurements were repeated a week after the primary analysis (except for the angular measurements) by both observers. The primary observer repeated all radiographic measurements in all the radiographic modalities a week after the primary analysis.

The second observer was requested to repeat the measurements for three skulls in each radiographic modality tested.

RESULTS

Statistical significance was elicited for all the overall mean differences between physical and radiographic distances (on PAN, CBCT, and PA) in both jaws. The panoramic overall mean distance differences in both jaws were overestimated (by 2.229 mm and 3.832 mm for maxilla and mandible, respectively). On the other hand, periapical radiographs' overall mean differences recorded underestimation of -3.707 mm in the maxilla and overestimation by 1.849 mm in the mandible. While both conventional two-dimensional modalities (i.e., PA and PAN) recorded mean differences exceeding a millimeter, CBCT, by contrast, provided the least submillimeter discrepancy in both, maxilla (M.D = -0.638 mm) and mandible (M.D = 0.326 mm).

In comparison to the overall mean difference, the statistical analysis of measurement differences acquired in each individual segment (point) did not elicit any statistical significance (between CBCT or PAN or PA vs. physical distances), except in the distance vertical (DV) of point P (R. maxilla) of the PA. Among all the investigated twenty-three individual points (segments), the mean differences between CBCT and physical distances were the least over the three modalities (Max. 2.047mm and Min. 0.127mm). The statistical analysis is further demonstrated in Tables 2 and 3.

Table 4 documents the differences between the linear and angular measurements (alveolar arc lengths), i.e., DUP/DLP, DUA/DLA. Of the 36 readings obtained, 21 of them exceeded the 1 mm (over or underestimating).

Comparison	PA (10 readings)	Pan (18 readings)	CBCT (23 readings)	
Discrepancy over 1 mm limit Discrepancy over 1 mm limit	9/10	16/18	4/23	
	Detailed de	scription of data		
Overestimation (>0mm)	5/10	17/18	11/23	
1axilla	0	8 R* [1.15-6.05 mm]	1 M* (0.22mm)	
landible	5 R* [1.27-2.52 mm]	9 R* [0.9-7.56mm]	10 R* [0.31-2.04mm]	
Inderestimation (<0mm)	5/10	1/18	12/23	
1axilla	5 R* [-0.83-5.57mm]	1 M* (-0.77)	8 R* [-0.15-(-1.8)mm]	
landible	0	0	4 R* [-0.4-(-0.92)mm]	

	Skull #	Right	side	Left side		
		DUP/DLP	DUA/DLA	DUP/DLP	DUA/DLA	
4	Maxilla	0,36	-5,04	0.95	-2,42	
1	Mandible	0,78	-3,48	-1,58	-3,88	
2	Mandible	0,25	0.84	0,04	-1,81	
3	Mandible	-0,78	-3,3	-3,08	-1,65	
4	Maxilla	-1,58	-0,44	-3,09	0.9	
	Mandible	-4,03	0.54	-0,33	-1,08	
5	Mandible	-2,61	-2,55	-0,05	-4,64	
6	Maxilla	0,34	-4,9	-0,8	-6,41	
	Mandible	-4,01	-2,8	-2,08	-0,24	
ar surement		at the linear measurements of difference (21 readings/36)	were bigger than angular o	ones and vice versa.		

Nonetheless, those 21 readings were all negative indicating that the angular measurements were more than the values of the linear ones (i.e., the linear physical distances underestimate their angular counterparts).

All measured distances showed excellent inter and intraexaminers reliability (using the intraclass correlation coefficient) except in three points (segments) which were poor, moderate, and good.

DISCUSSION

Despite the statistical significance elicited for the overall measurement discrepancies between physical vs. all radiographic modalities compared, clinically significant distortions were only attained from periapical and panoramic measurements. The discrepancy of measurements was inconsistent with the numerous anatomical segments investigated. In this investigation, it was noted that the reliability of the radiographic dimensions was highly influenced by the radiographic position during periapical and panoramic radiographic examinations. While the current investigation was performed under simulated clinical settings, such an approach may not be constantly achieved in an ordinary, everyday clinical environment. A submillimeter radiographic measurement discrepancy on CBCT volumes mentioned to be clinically insignificant.^{24,25,26} Although we accept this small margin of error, it is challenging to consider the clinical significance of this minute discrepancy when related to the spatial location of vital structures, it can mean the difference between success and failure.

CBCT technique was reported to provide highly precise dimensions of the studied anatomical structures. ^{5-7,26-28} Within a high overall accuracy, slight measurement overestimation ^{25,29,30} and underestimation ^{7,31-33} were mentioned. ²⁶ Consequently, during the planning of surgical procedures, a safety zone of 2 mm still applies. ²⁶ The current investigation concurs with the previous reports regarding the accuracy of CBCT while revealing an overall submillimeter accuracy (-0.638, 0.326mm for maxilla and mandible, respectively). Nevertheless, CBCT volumes showed an over-millimetre discrepancy in the vertical distance (DV) at 3 individual mandibular sites [1.18mm - 2.04mm] and one in the maxilla (-1.8mm).

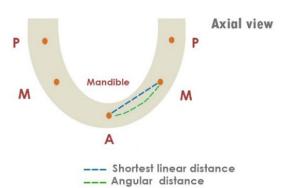
Multiple factors may impact the accuracy of CBCT measurements e.g. the imposed artefacts (like beam hardening and motion artefacts), exposure settings, and the software used.²⁶ The head position does not affect the CBCT

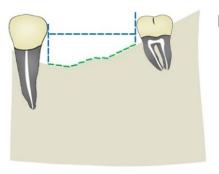
volume accuracy.^{34,35} However, generating cross-sectional images based on an inaccurate and unsynchronized (radiographically and physically) virtual orientation of the head (particularly the sagittal tilting) might lead to inaccurate measurements if transferred to the patient's mouth, as it affects the height of subsequent cross-sections.³⁶ Some dimensional discrepancies discovered at the surgical setting are a result of the erroneous transfer of virtually performed measurements on the cross-sectional slices.³⁷ We, therefore, highlight the importance of accurate identification and synchronization of reference landmarks (radiographically and clinically).

The reproducibility of 2D radiographic linear measurements of 3D physical structures is the most likely source of discrepancies (Figure 4). The shortest linear distance measured (physically) between two segments (points) was -in general- less than the angular counterpart which was measured with the cord placed directly on the alveolar ridge. Such a finding should be considered clinically while performing "free-hand" implantology, and a reference measurement mark point to the drilling site need to be reproduced in the patient's jaw.

While possible magnification and inherent distortions are the main disadvantages, panoramic radiographs are a common radiographic procedure that offers a wide range of advantages. ^{1,38} Multiple reports indicated dimensional reliability and beneficial use of these radiographs especially in the posterior segments of the jaws; ^{3,10,13-18,39} yet, opposing evidence also exist. ¹⁹⁻²³ Compared to our findings, the overall measurement discrepancies exceeded the 1 mm range in maxilla and mandible (2.229, 3.832 mm, respectively), indicating overall inferior accuracy. Out of 18 panoramic individual points measurements, the mean difference was over 1 mm in 16 locations in maxilla and mandible, overestimated (>0 mm) in 17 readings [1.15 – 7.56 mm], and underestimated (>0 mm) in one reading (-0.77 mm).

Comparable findings were noted in periapical radiographs measurements where overall measurement discrepancies of -3.707 for maxilla and 1.849mm for mandible were found. Mandibular measurements showed less discrepancy – although >1 mm- compared to maxillary ones. Although performed in a simulated ideal setting, anatomical variations (e.g., ridge inclination, shallow palate) in the maxilla may readily cause distortions, as ideal parallelism between the axis of the alveolar ridge and the x-ray receiver was challenging. In mandible and excluding the





Lateral view

Figure 4. Illustration of the assumed angular distances between various jaw segments (Reprinted from Beshtawi, 2021).40

muscle repulsion (which may occur in real patients) in the floor of the mouth, achieving ideal parallelism was unchallenging and was translated in reduced measurement discrepancies in the mandible compared to the maxilla. Though PA showed accurate individual dimensions at multiple anatomical sites, the accuracy was inconsistent throughout the analysis. As a result, accurate reproduction of the anatomical structures may not be guaranteed in every clinical setting.

CONCLUSIONS

Compared to panoramic and periapical radiographs, CBCT achieved superior sub-millimeter accuracy in the maxilla and mandible. Measurements done at the maxillary sites showed more accuracy compared to the mandibular sites on panoramic radiographs, however, the highest discrepancy values were noted in the anterior regions. In contrast, the opposite was noted on periapical radiographs examinations i.e., measurements obtained from the mandible revealed better accuracy than the maxillary sites. While panoramic and periapical radiographs exhibited individual accurate measurements, the overall differences indicate inferior dimensional accuracy compared with CBCT. In this paper, the accuracy of the CBCT modality is verified and thus is recommended for implant planning.

Limitations

Angular measurements were not repeated for inter- and intra- observers' agreements.

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References

- Tyndall DA, Price JB, Tetradis S, Ganz SD, Hildebolt C, Scarfe WC, et al. Position statement of the American Academy of Oral and Maxillofacial Radiology on selection criteria for the use of radiology in dental implantology with emphasis on cone beam computed tomography. Oral Surg Oral Med Oral Pathol Oral Radiol. 2012 Jun; 113(6): 817-26.
- Vazquez L, Saulacic N, Belser U, Bernard JP. Efficacy of panoramic radiographs in the preoperative planning of posterior mandibular implants: A prospective clinical study of 1527 consecutively treated patients. Clin Oral Implants Res. 2008; 19(1): 81-5.
- Assaf M, Gharbyah A. Accuracy of Computerized Vertical Measurements on Digital Orthopantomographs: Posterior Mandibular Region. J Clin Imaging Sci. 2014; 4(2):7.
- Bornstein MM, Horner K, Jacobs R. Use of cone beam computed tomography in implant dentistry: current concepts, indications and limitations for clinical practice and research. Vol. 73, Periodontology 2000. Blackwell Munksgaard. 2017; 51-72.
- Moshfeghi M, Tavakoli MA, Hosseini ET, Hosseini AT, Hosseini IT. Analysis of linear measurement accuracy obtained by cone beam computed tomography (CBCT-NewTom VG). Dent Res J (Isfahan). Dec 2012; 9(Suppl 1): S57-62.
- Stratemann SA, Huang JC, Maki K, Miller AJ, Hatcher DC. Comparison of cone beam computed tomography imaging with physical measures. Dentomaxillofacial Radiol. 2008; 37(2): 80-93.
- Luangchana P, Pornprasertsuk-Damrongsri S, Kiattavorncharoen S, Jirajariyavej B. Accuracy of Linear Measurements Using Cone Beam Computed Tomography and Panoramic Radiography in Dental Implant Treatment Planning. Int J Oral Maxillofac Implants. 2015; 30(6): 1287-94.
- Flügge T, Derksen W, te Poel J, Hassan B, Nelson K, Wismeijer D. Registration of cone beam computed tomography data and intraoral surface scans – A prerequisite for guided implant surgery with CAD/CAM drilling guides. Clin Oral Implants Res. Sep 2017; 28(9): 1113-8.
- Nagalaxmi V, Swetha P, Srikanth K, Lalitha CH. Implant imaging: A review of literature. IJSS Case Reports Rev. 2015; 2(5): 48-54.
- Özalp Ö, Tezerisener HA, Kocabalkan B, Büyükkaplan US, Özarslan MM, Kaya GS, et al. Comparing the precision of panoramic radiography and cone-beam computed tomography in avoiding anatomical structures critical to dental implant surgery: A retrospective study. Imaging Sci Dent. 1 Dec 2018; 48(4): 269-75.
- Ganguly R, Ruprecht A, Vincent S, Hellstein J, Timmons S, Qian F. Accuracy of linear measurement in the Galileos cone beam computed tomography under simulated clinical conditions. Dentomaxillofacial Radiol. 2011; 40(5): 299-305.
- Nikneshan S, Aval SH, Bakhshalian N, Shahab S, Mohammadpour M, Sarikhani S. Accuracy of linear measurement using cone-beam computed tomography at different reconstruction angles. Imaging Sci Dent. 2014; 44(4): 257-62.
- Amarnath GS, Kumar U, Hilal M, Muddugangadhar BC, Anshuraj K, Shruthi CS. Comparison of cone beam computed tomography, orthopantomography with direct ridge mapping for pre-surgical planning to place implants in cadaveric mandibles: An ex-vivo study. J Int oral Heal. 2015; 7 (Suppl 1): 38-42.
- Zarch S, Bagherpour A, Javadian Langaroodi A, Ahmadian Yazdi A, Safaei A. Evaluation of the accuracy of panoramic radiography in linear measurements of the jaws. Iran J Radiol. 2011; 8(2): 97-102.
- 15. Hu KS, Choi DY, Lee WJ, Kim HJ, Jung UW, Kim S. Reliability of two different presurgical preparation methods for implant dentistry based on panoramic radiography and cone-beam computed tomography in cadavers. J Periodontal Implant Sci. 2012 Apr; 42(2): 39-44.

- 16. Pertl L, Gashi-Cenkoglu B, Reichmann J, Jakse N, Pertl C. Preoperative assessment of the mandibular canal in implant surgery: comparison of rotational panoramic radiography (OPG), computed tomography (CT) and cone beam computed tomography (CBCT) for preoperative assessment in implant surgery. Eur J Oral Implantol. 2013; 6(1): 73-80.
- Kim YK, Park JY, Kim SG, Kim JS, Kim JD. Magnification rate of digital panoramic radiographs and its effectiveness for preoperative assessment of dental implants. Dentomaxillofacial Radiol. 2011; 40(2): 76-83.
- Vazquez L, Nizamaldin Y, Combescure C, Nedir R, Bischof M, Dohan Ehrenfest DM, et al. Accuracy of vertical height measurements on direct digital panoramic radiographs using posterior mandibular implants and metal balls as reference objects. Dentomaxillofacial Radiol. 2013; 42(2).
- Bou Serhal C, Jacobs R, Flygare L, Quirynen M, Van Steenberghe D. Perioperative validation of localisation of the mental foramen. Dentomaxillofacial Radiol. 2002; 31(1): 39-43.
- Correa LR, Spin-Neto R, Stavropoulos A, Schropp L, da Silveira HED, Wenzel A. Planning of dental implant size with digital panoramic radiographs, CBCT-generated panoramic images, and CBCT cross-sectional images. Clin Oral Implants Res. 2014; 25(6): 690-5.
- Bertram F, Bertram S, Rudisch A, Emshoff R. Assessment of location of the mandibular canal: Correlation between panoramic and cone beam computed tomography measurements. Int J Prosthodont. 2018; 31(2): 129-34.
- 22. Haghnegahdar A, Bronoosh P. Accuracy of linear vertical mea surements in posterior mandible on panoramic view. Dent Res J (Isfahan). 2013; 10(2): 220-4.
- Dudhia R, Monsour PA, Savage NW, Wilson RJ. Accuracy of angular measurements and assessment of distortion in the mandibular third molar region on panoramic radiographs. Oral Surgery, Oral Med Oral Pathol Oral Radiol Endodontology. 2011; 111(4): 508-16.
- Torres MGG, Campos PSF, Segundo NPN, Navarro M, Crusoé-Rebello I. Accuracy of linear measurements in cone beam computed tomography with different voxel sizes. Implant Dent. 2012 Apr; 21(2): 150-5.
- 25. Kobayashi K, Shimoda S, Nakagawa Y, Yamamoto A. Accuracy in measurement of distance using limited cone-beam computerized tomography. Int J Oral Maxillofac Implants. 2004; 19(2): 228-31.
- Fokas G, Vaughn VM, Scarfe WC, Bornstein MM. Accuracy of linear measurements on CBCT images related to presurgical implant treatment planning: A systematic review. Clin Oral Implants Res. 2018; 29 (Suppl 16): 393-415.
- 27. Ganguly R, Ramesh A, Pagni S. The accuracy of linear measurements of maxillary and mandibular edentulous sites in conebeam computed tomography images with different fields of view and voxel sizes under simulated clinical conditions. Imaging Sci Dent. 2016; 46(2): 93-101.
- De Andrade J, Valerio C, Monteiro M, Machado V, Manzi F. Comparison of 64-detector-multislice and cone beam computed tomographies in the evaluation of linear measurements in the alveolar ridge. Int J Prosthodont. 2016; 29(2): 132-4.
- Al-Ekrish AA, Ekram M. A comparative study of the accuracy and reliability of multidetector computed tomography and cone beam computed tomography in the assessment of dental implant site dimensions. Dentomaxillofacial Radiol. 2011; 40(2): 67-75.
- Luk LCK, Pow EHN, Li TKL, Chow TW. Comparison of ridge mapping and cone beam computed tomography for planning dental implant therapy. Int J Oral Maxillofac Implants. 2011; 26(1): 70-4.
- 31. Sheikhi M, Dakhil-Alian M, Bahreinian Z. Accuracy and reliability of linear measurements using tangential projection and cone beam computed tomography. Dent Res J (Isfahan). 2015; 12(3): 271-7.

- Baumgaertel S, Palomo JM, Palomo L, Hans MG. Reliability and accuracy of cone-beam computed tomography dental measurements. Am J Orthod Dentofac Orthop. 2009; 136(1): 19-25.
- Lascala CA, Panella J, Marques MM. Analysis of the accuracy of linear measurements obtained by cone beam computed tomography (CBCT-NewTom). Dentomaxillofacial Radiol. Sep 2004; 33(5): 291-4.
- 34. Adibi S, Shahidi S, Nikanjam S, Paknahad M, Ranjbar M. Influence of Head Position on the CBCT Accuracy in Assessment of the Proximity of the Root Apices to the Inferior Alveolar Canal. J Dent (Shiraz, Iran). 2017; 18(3): 181-6.
- El-Beialy AR, Fayed MS, El-Bialy AM, Mostafa YA. Accuracy and reliability of cone-beam computed tomography measurements: Influence of head orientation. Am J Orthod Dentofac Orthop. 2011; 140(2): 157-65.
- 36. Mora MA, Chenin DL, Arce RM. Software tools and surgical guides in dental-implant-guided surgery. Dent Clin North Am. 2014; 58(3): 597-626.
- 37. Harris D, Horner K, Gröndahl K, Jacobs R, Helmrot E, Benic GI, et al. E.A.O. guidelines for the use of diagnostic imaging in implant dentistry 2011. A consensus workshop organized by the European Association for Osseointegration at the Medical University of Warsaw. Clin Oral Implants Res. Nov 2012; 23(11): 1243-53.
- Shah N, Bansal N, Logani A. Recent advances in imaging technologies in dentistry. World J Radiol. 28 Oct 2014; 6(10): 794-807.
- 39. Kayal R. Distortion of digital panoramic radiographs used for implant site assessment. J Orthod Sci. 2016; 5(4): 117-20.
- Beshtawi K. Recommendations for the development of a framework for radiological imaging studies during implant therapy in SA. University of the Western Cape. 2021. Available from: http://hdl.handle.net/11394/7744.